

## Roskilde University

#### High-dose etoposide formulations do not saturate intestinal P-glycoprotein

Development, stability, and pharmacokinetics in Sprague-Dawley rats

Al-Ali, Ahmed A.Abdulhussein; Sandra, Louis; Versweyveld, Dries; Pijpers, Ils; Dillen, Lieve; Vermeulen, An; Snoeys, Jan; Holm, René; Nielsen, Carsten Uhd

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- 4 Ahmed A. Abdulhussein Al-Alia, Louis Sandrab, Dries Versweyveldc, Ils Pijpersd, Lieve Dillend,
- 5 An Vermeulen<sup>b</sup>, Jan Snoeys<sup>d</sup>, René Holm<sup>e,f</sup>, and Carsten Uhd Nielsen<sup>a\*</sup>

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- <sup>a</sup>: Department of Physics, Chemistry and Pharmacy, University of Southern Denmark, Campusvej 55,
- 8 DK-5230 Odense M, Denmark
- 9 b: Quantitative Sciences, Janssen R&D, a division of Janssen Pharmaceutica NV, Turnhoutseweg 30,
- 10 2340 Beerse, Belgium
- <sup>c</sup>: Non Clinical Safety, Janssen R&D, a division of Janssen Pharmaceutica NV, Turnhoutseweg 30,
- 12 2340 Beerse, Belgium
- d: Drug Metabolism and Pharmacokinetics (DMPK), Janssen R&D, a division of Janssen
- 14 Pharmaceutica NV, Turnhoutseweg 30, 2340 Beerse, Belgium
- 15 e: Drug Product Development, Janssen R&D, a division of Janssen Pharmaceutica NV,
- 16 Turnhoutseweg 30, 2340 Beerse, Belgium
- 17 f: Department of Science and Environment, Roskilde University, 4000 Roskilde, Denmark
- \*: Corresponding author at: Department of Physics, Chemistry and Pharmacy, University of Southern
- Denmark, Campusvej 55, DK-5230 Odense M, Denmark. Phone: +45 6550 9427 e-mail: cun@sdu.dk

Abstract: It has been suggested that oral absorption of low-permeable P-glycoprotein (P-gp) substrates can be increased through saturation of P-gp. For BCS class IV drug substances, saturating P-gp is challenging due to low aqueous solubility. The present study investigated if the BCS IV drug substance etoposide could be solubilized to a concentration saturating P-gp after oral administration. A formulation consisting of 10% (w/v) of pluronic® F-127 and polyvinylpyrrolidone/vinyl acetate (PVP/VA), and 57% (v/v) ethanol enhanced etoposide's solubility approximately 100 times (16 mg mL-1) compared to its aqueous solubility. *In vitro*, this formulation was stable upon dilution in simulated intestinal fluid. In male Sprague-Dawley rats, oral administration of increasing solubilized etoposide doses using the formulation matrix increased the AUC<sub>0-∞</sub> of etoposide dose-proportionally but resulted in a lower absolute oral bioavailability (F) and rate of absorption as compared to control. At the highest investigated dose (100 mg kg<sup>-1</sup>), AUC<sub>0-∞</sub> and  $C_{max}$  were significantly increased by 2.9-and 1.4-fold, respectively, compared to control dosed at 20 mg kg<sup>-1</sup>. A single oral dose of 20 mg kg<sup>-1</sup> zosuquidar followed by 20 mg kg<sup>-1</sup> oral etoposide increased F 8.6-fold. In conclusion, a stable formulation with improved etoposide solubility was developed, yet the formulation did not result in increased oral bioavailability of etoposide.

**Keywords:** P-glycoprotein, Etoposide, Zosuquidar, Population pharmacokinetics, Sprague-Dawley rats.

#### 1. Introduction:

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P-glycoprotein (P-gp, MDR1) has been shown to limit the intestinal absorptive permeability of lowpermeable substrates in cell cultures (Alsenz et al., 1998; Collett et al., 1999; Sparreboom et al., 1997; Terao et al., 1996; Troutman and Thakker, 2003b). *In vivo*, in wild type (WT) rats, P-gp restricts the oral bioavailability of several P-gp substrates such as loperamide (Zamek-Gliszczynski et al., 2012), paclitaxel (Zamek-Gliszczynski et al., 2012), digoxin (Nielsen et al., 2016), and etoposide (Al-Ali et al., 2018a). This is evident since the oral bioavailability is significantly increased in mdr1a deficient rats (Al-Ali et al., 2018a; Nielsen et al., 2016; Zamek-Gliszczynski et al., 2012). Moreover, coadministration of P-gp substrates with potent small-molecular P-gp inhibitors such as verapamil (Tsuruo et al., 1981), dexverapamil (Gramatté and Oertel, 1999), valspodar (PSC-833) (Mayer et al., 1997; van Asperen et al., 1997), or zosuguidar (LY335979) (Bardelmeijer et al., 2004) increased the oral bioavailability of the substrates in preclinical studies. However, using inhibitors to increase the oral bioavailability of P-gp substrates in some cases also affects metabolism via the cytochrome P450s and results in adverse effects (Breedveld et al., 2006; Palmeira et al., 2012; Varma et al., 2003; Varma and Panchagnula, 2005). Other studies have shown that co-administration of pharmaceutical excipients such as nonionic surfactants may also have the potential to increase the oral bioavailability of digoxin (Cornaire et al., 2004; Nielsen et al., 2016; Zhang et al., 2003), etoposide (Akhtar et al., 2017; Al-Ali et al., 2018a), and paclitaxel (Varma and Panchagnula, 2005) in WT rats. To overcome the cellular efflux mediated by P-gp to increase intestinal absorption, it should in theory be possible to saturate the transporters by achieving intestinal concentrations well above the K<sub>m</sub>-value for the substrate-transporter binding as mentioned by e.g. Lin and Yamazaki (Lin and Yamazaki, 2003). Taking into consideration the degree of passive diffusion, intestinal metabolism, and P-gp substrate binding affinity, this may be a feasible strategy for drug substances with sufficient aqueous solubility, low passive diffusion, and limited metabolism. The experimental evidence for the feasibility of

saturating P-gp in the intestine through a pharmaceutical formulation strategy is however relatively limited and ambiguous. Lin and Yamazaki and Chiou et al., retrospectively, interpreted the pharmacokinetic human studies of the BCS II compound talinolol made by de Mey et al., and concluded that since the dose normalized AUC values after oral administration of increasing talinolol doses increased with higher doses, this suggested saturation of P-gp efflux (Chiou et al., 2001; de Mey et al., 1995; Lin and Yamazaki, 2003). Talinolol is also a substrate of absorptive solute carriers including organic anion transporting polypeptide 1A2 (OATP1A2) and OATP2B1 (Shirasaka et al., 2010) making the absorption kinetics quite complicated. Since high doses of a P-gp substrate are needed to saturate the transporter, and as most P-gp substrates are poorly water-soluble substances (Wang et al., 2001), suitable pharmaceutical formulation approaches are required to solubilize the substrate. SMEEDs formulations could be used, but they often contain surfactants that are also P-gp inhibitors see e.g. Zhao et al. (Zhao et al., 2013). Thus, in the present study a formulation that can maintain the substrate in a solubilized-form upon dilution in the intestinal lumen without P-gp inhibiting surfactants was developed using etoposide a BCS class IV P-gp substrate. Etoposide was selected since intestinal P-gp limited oral etoposide bioavailability in WT rats, whereas etoposide was completely absorbed in *mdr1a* deficient rats (Al-Ali et al., 2018a). Moreover, data suggests that Bcrp has very little impact on the intestinal absorption of etoposide in mice (Allen et al., 2003). A formulation was designed with ethanol and surfactant to enhance the solubility of etoposide. Etoposide has a low aqueous solubility of 0.15-0.2 mg mL<sup>-1</sup> (Beig et al., 2015; Darwish et al., 1989) and since 10% ethanol significantly enhanced etoposide stability in artificial intestinal fluid, ethanol was used as a solubilizing co-solvent for etoposide (Joel et al., 1995). Since many nonionic surfactants inhibit P-gp in vitro (Al-Ali et al., 2019; Al-Ali et al., 2018b; Batrakova et al., 1999; Batrakova et al., 2003; Gurjar et al., 2018; Li-Blatter et al., 2012; Lo, 2003; Zhao et al., 2016) and in vivo (Akhtar et al., 2017; Al-Ali et al., 2018a; Ma et al., 2011; Nielsen et al., 2016; Zhao

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et al., 2013), a surfactant without P-gp inhibiting properties was chosen to evaluate the effect of increasing the dose of etoposide without a potential surfactant mediated P-gp inhibitory effect. Previous *in vitro* studies have reported that pluronic® F-127 did not inhibit the P-gp-mediated efflux of several substrates e.g. rhodamine 123 (Al-Ali et al., 2019; Batrakova et al., 2003; Wei et al., 2013), nelfinavir (Shaik et al., 2008), digoxin (Gurjar et al., 2018), and etoposide (Al-Ali et al., 2018a), hence this surfactant was chosen. Polyvinylpyrrolidone-vinyl acetate (PVP/VA) was suggested as a potential precipitation inhibitor (Kalaiselvan et al., 2006; Knopp et al., 2016; Xu and Dai, 2013) and formulation stabilizer during storage (Knopp et al., 2016; Prudic et al., 2014), thus it was included in the formulation.

The aim of the present study was to prepare an oral formulation of high concentration of etoposide and to investigate the stability on storage, and upon dilution in fasted state simulated intestinal fluid (FaSSIF). Furthermore, the formulation was used to investigate if the systemic exposure of orally administered etoposide in rats could be increased through saturation of P-gp transport activity.

#### 2. Material and methods:

#### 2.1. Materials

Caco-2 cells were obtained from the American Type Culture Collection (ATCC). Cell culture media and Hanks balanced salt solution (HBSS) were obtained from Life Technologies (Høje-Taastrup, Denmark). Etoposide (>99% purity) was purchased from Selleckchem (Munich, Germany). Sodium chloride, sodium taurocholate, sodium hydroxide, potassium chloride, L-α-phosphatidylcholine (approx. 60%), potassium phosphate monobasic (≥97%), and pluronic<sup>®</sup> F-127 suitable for cell culture, 2-(N-morpholino) ethane sulfonic acid (MES), N-[2-Hydroxyethyl] piperazine N'-[2-ethanesulfonate] (HEPES), verapamil, digoxin, and bovine serum albumin (BSA) were from Sigma

(Brøndby, Denmark). Ethanol (99.5 %) was from VWR Chemicals (Fontenay-sous-Bois, France). Polyvinylpyrrolidone-vinyl acetate (Kollidon® VA 64, referred as PVP/VA) meets Ph. Eur. standards and was from BASF SE (Ludwigshafen, Germany). Transwell® inserts with polycarbonate membrane (0.4 μm pore size, 1.12 cm²) were from Corning Life Sciences and purchased through Sigma Aldrich (Brøndby, Denmark). Whatman® Nuclepore™ Track-Etched Membranes (0.03 μm pore-size, 19 mm in diameter) were purchased from Sigma Aldrich (Brøndby, Denmark). LOCTITE® 401 glue was purchased from RS Components Ltd. (Corby, UK). ³H-etoposide (specific activity 700 mCi mmol¹) was from Moravek (CA, USA). ¹⁴C-glycine (specific activity 87 mCi mmol¹) was purchased from Larodan (Solna, Sweden) and ¹⁴C-mannitol with a specific activity of 51.50 mCi/mmol was from Sigma Aldrich (Brøndby, Denmark). Ultima Gold liquid was purchased from Perkin Elmer (Skovlunde, Denmark). The radio-chemical purity of the isotopes was greater than 97%.

#### 2.2. Cell culture and transport experiments

Caco-2 cells were cultured as previously described by Nielsen and co-workers (Nielsen et al., 2001). Briefly, cells were seeded in culture flasks and passaged in Dulbecco's Modified Eagle's medium (DMEM) supplemented with 10 % fetal bovine serum, penicillin/streptomycin (100 U ml<sup>-1</sup> and 100 ug ml<sup>-1</sup>, respectively), 1 % L-glutamine, and 1 % non-essential amino acids. Cells were seeded onto tissue culture treated Transwells (1.0 cm<sup>2</sup>, 0.4 µm pore size) at a density of 10<sup>5</sup> cells cm<sup>-2</sup>. Transepithelial electrical resistance (TEER) at room temperature was measured before the experiment. All TEER values of monolayers used were >400  $\Omega$  cm<sup>2</sup>. Transport experiments were performed on day 24-28 after seeding. 

HEPES buffers adjusted to pH 7.4. The concentration of etoposide on the donor (cis) side was 20 –

Apical (A) to basolateral (B) and B to A fluxes of tritium labeled etoposide was measured in 10 mM

520 μM. Samples (20 μl) were taken from the donor solution at t=0 and 210 min and 150 μl samples were taken from the receiver solution and replaced with fresh buffer (t=30, 60, 90, 120, 150, 180, and 210 min). The transport of <sup>3</sup>H-etoposide was also measured in the presence of 100 µM of digoxin and 50 µM verapamil on both donor and receiver side, respectively. Samples were transferred to scintillation vials, where 2 ml of scintillation fluid was added and the radioactivity was counted in a liquid scintillation analyzer. Fluxes were constant after 60 min. The steady state flux values were thus obtained as the means of the flux values between 90-210 min. After the experiment, the integrity of the Caco-2 cell monolayers was evaluated by <sup>14</sup>C-mannitol transport studies. Samples were taken from the donor chamber (10 µl) at 20, 40, and 60 min, and from the receiver chamber at 0, 20, 40, and 60 min. The permeability (Papp) of mannitol was unaffected by etoposide, digoxin and verapamil and had a  $P_{app}$  value of 1.4  $10^{-06} \pm 4.2 \ 10^{-07} \ cm \ s^{-1}$ . The transport across the filter without Caco-2 cells was investigated in order to assess whether the filter was a barrier to diffusion of etoposide. The permeability across the filter was calculated using non-steady state kinetics and had a value of 3.1 10<sup>-1</sup>  $^{04} \pm 4.2 \ 10^{-05} \ \text{cm s}^{-1}$ . The P-gp dependent flux (J<sub>P-gp</sub>) was calculated similarly to described by Troutman and Thakker (Troutman and Thakker, 2003a), where the total flux of etoposide was subtracted with the flux of etoposide in the presence of 100 µM of digoxin and 50 µM verapamil to yield the concentration dependent effect of P-gp on etoposide transport. Here we used Caco-2 cells from ATCC, and proteomics data suggest that BCRP expression is very low in the substrain compared to Caco-2 cells obtained from The European Collection of Authenticated Cell Cultures (ECACC) or/and Deutsche Sammlung von Mikroorganismen und Zellkulturen (DSMZ), as reviewed in Al-Ali et al., 2019 (Al-Ali et al., 2019). In Caco-2 cells from DSMZ it has been shown that 25 µM zosuquidar abolish polarized etoposide transport completely (Nielsen et al., 2020), while it has also been shown that

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verapamil completely abolishes polarized etoposide in Caco-2 cells (Mo et al., 2011). Therefore, it seems likely that in Caco-2 cells from ATCC BCRP has a minor impact on etoposide transport.

The resulting etoposide flux in the B-A direction was then fitted to the following equation:

$$J_{P-gp} = \frac{J_{P-gp,\max*C_d}}{K_{m,app} + C_d} \tag{1}$$

where,  $J_{P-gp}$  is the P-gp mediated flux,  $J_{P-gp,max}$  is the maximal flux,  $K_{m,app}$  is the apparent Michaelis constant and  $C_d$  is the donor concentration.

#### 2.3. Animals

In vivo pharmacokinetic studies were performed in WT male Sprague-Dawley rats, which were from Charles River Laboratories (Sulzfeld, Germany). The study protocol was approved by the local ethical committee in accordance with EC Directive 2010/63/EU and Belgian Law/1991 for Protection of Vertebrate Animals used for Experimental and other Scientific Purposes. The rats were received one week prior to the *in vivo* experiments, acclimatized and maintained on standard feed conditions with free access to water. The animals were fasted for 16 h before the pharmacokinetic studies. During the experiments, the rats had free access to water, but not food. At the day of the experiment, the weight of the animals was 242-275 g.

### 2.4. Preparation of etoposide-containing formulations

Different formulations of etoposide were prepared using the nonionic surfactant pluronic<sup>®</sup> F-127, the copolymer PVP/VA, ethanol, and ultra-purified water (Table 1). Pluronic<sup>®</sup> F-127 was first dissolved in 57% (v/v) ethanol solution at room temperature. Etoposide was then added to the surfactant-

containing solution and placed in a water bath at 40° C for 15-30 min, before the solution was mixed using a magnetic stirrer for 15-30 min. The solution was visually inspected for undissolved particles. PVP/VA powder was subsequently added, and the mixture placed in a water bath at 37° C for 15-30 min, before being mixed using a magnetic stirrer for 15-30 min. The solution was again visually investigated for undissolved particles. Finally, provided that the etoposide-containing formulation was clear, the formulation was transferred to a glass container, protected from light, and kept at room temperature overnight (approx. 15 h). If no sign of precipitation appeared after 15 h, the formulation was further investigated for precipitation upon dilution with FaSSIF, see details below.

2.5. Monitoring of etoposide containing-formulations diluted with fasted state simulated intestinal fluid

Monitoring that etoposide does not precipitate in the different formulations when diluted with FaSSIF was investigated as previously described by Al-Ali et al. (Al-Ali et al., 2018a). Briefly, FaSSIF was prepared according to Galia et al., composed of 0.39 g potassium phosphate monobasic, 0.77 g potassium chloride, 3 mM sodium taurocholate, 0.75 mM L- $\alpha$ -phosphatidylcholine, and ultra-purified water added to 100 mL (Galia et al., 1998). The pH was then adjusted to  $6.50 \pm 0.05$  with sodium hydroxide before the osmolality was adjusted to  $270 \pm 10$  mOsm kg<sup>-1</sup> using sodium chloride (Galia et al., 1998). The different formulations of etoposide were then added to FaSSIF in a ratio of 1:2 (formulation:FaSSIF) to simulate the likely intestinal dilution in the rats (McConnell et al., 2008) and monitored for two hours by measuring the absorbance at 400 nm and 25° C every 10 min using a UV-spectrophotometer (Genesys 10-S from Thermo Fisher Scientific (WI, USA)). Before each measurement, solutions were mixed for 10 seconds using pipetting.

#### 2.6. Dialysis studies investigating etoposide release from different formulations

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Dialysis studies were designed and optimized as previously described by Al-Ali et al., (Al-Ali et al., 2018a), with minor modifications. In brief, the dialysis setup allows the diffusion of free-fraction of etoposide (unbound to micelles) and retains etoposide-bound to micelles, which should be not diffused across a 0.03 µm pore-size polycarbonate membrane during the course of the experiment (2 h). Polycarbonate membranes (0.03 µm pore size, 19 mm in diameter) were attached to Transwell holders (1.12 cm<sup>2</sup>) by LOCTITE® 401 glue and left to dry at room temperature overnight (Al-Ali et al., 2018a). The Transwell inserts, with attached polycarbonate membranes, were then hydrated overnight in ultra-purified water. On the day of the experiment, Transwell inserts with polycarbonate membranes were first pre-incubated with HBSS supplemented with 10 mM HEPES and adjusted to pH 7.40  $\pm$  0.05 (HBSS<sup>+</sup>) on a shaking plate at 220 rpm at 37° C for 10 min. Donor solutions of <sup>3</sup>Hetoposide and <sup>14</sup>C-glycine were prepared in HBSS<sup>+</sup> (Control), or in different formulation-matrices containing 10% (w/v) PVP/VA, 57% (v/v) ethanol, and pluronic® F-127 at 1.5, 3 or 10%, referred to as Matrix-PF127 1.5%, Matrix-PF127 3%, or Matrix-PF127 10%, respectively, or mixed with a formulation with the highest concentration of etoposide. This formulation contained 15-16 mg mL<sup>-1</sup> etoposide, 10% (w/v) of pluronic® F-127 and PVP/VA, and 57% (v/v) ethanol. The solution containing radioactive compounds was then added to FaSSIF at a 1:2 ratio to achieve final concentrations of <sup>3</sup>H-etoposide and <sup>14</sup>C-glycine at 0.25 µCi mL<sup>-1</sup>, 0.36 µM and 0.25 µCi mL<sup>-1</sup>, 2.87 μM, respectively, before these isotopes-containing solutions (500 μL) were added to the upper side of the polycarbonate membrane. Experiments started when receiver-release media (1650 µL) was loaded in the lower side of the polycarbonate membrane. Receiver-release media consisted of HBSS buffer supplemented with 10 mM HEPES and adjusted to pH  $6.50 \pm 0.05$  for all conditions except for the formulation containing the highest concentration of etoposide where the medium was the matrix of this formulation (i.e. 10% of pluronic® F-127 and PVP/VA, and 57% ethanol without

etoposide) in order to prevent etoposide precipitation when accumulated in the receiver chamber. Experiments were performed at 37° C and shaking mode 220 rpm. Donor samples were collected at 0, 60 and 120 min, while receiver samples were collected at 15, 30, 60, 90, and 120 min. Receiver-release medium was replaced at each sampling occasion in order to preserve the sink condition. Finally, Ultima Gold scintillation fluid (2 mL) was added to every sample, vortexed for one minute and counted for 10 min on a scintillation counter (TriCarb 4910TR) from Perkin Elmer, USA.

#### 2.7. Pharmacokinetic study in wild-type male Sprague-Dawley rats

The rats were randomly assigned to receive different doses of etoposide in ethanol solution or in a formulation matrix consisting of 10% (w/v) pluronic® F-127 and PVP/VA, 57% (v/v) ethanol, and ultra-purified water. For intravenous administration, the rats received etoposide solution (2.86 mg mL<sup>-1</sup> in 57% v/v ethanol) at a dose of 5 mg kg<sup>-1</sup> etoposide. Administration volume was adjusted to 2 mL with water before dosing the rats. For oral administration by oral gavage, the control group received an etoposide solution (2.86 mg mL<sup>-1</sup> in 57% v/v ethanol) at a dose of 20 mg kg<sup>-1</sup> etoposide and a dosing volume of 7 mL kg<sup>-1</sup>. In the positive control group, the rats received a zosuquidar solution (2 mg mL<sup>-1</sup>) at a dose of 20 mg kg<sup>-1</sup> and dosing volume of 10 mL kg<sup>-1</sup>, 30 min before the administration of etoposide doses which were administered in a similar fashion to the control group. For oral administration of increasing doses of etoposide, an increasing concentration of etoposide was solubilized in the formulation matrix i.e. 2.86, 7.15 and 14.3 mg mL<sup>-1</sup>. These etoposide-containing formulations were administered at doses of 20, 50, and 100 mg kg<sup>-1</sup>, respectively, in a dosing volume of 7 mL kg<sup>-1</sup>. Each dosing group consisted of 5-6 male Sprague-Dawley rats. After oral or intravenous administration of etoposide, blood samples were collected at 0.25, 0.5, 0.75, 1, 2, 3, 4, and 6 h, as well as at 5 min (0.0833 h) post intravenous administration of etoposide. The samples were obtained

at each sampling point by puncturing the lateral tail vein using a 23G needle and approximately 35  $\mu$ L of blood were collected using a capillary tube from VITREX Medical A/S (Herlev, Denmark). The capillaries with samples were then sealed with VITREX Sigillum Wax. Plasma samples were harvested immediately from these capillaries after centrifugation at 1900xg for 10 min at 4°C and transferred to a 10  $\mu$ L end-to-end capillary (VITREX) followed by storage at -20°C until further bioanalysis. At 6 h, the last samples were collected, and the animals were euthanized.

### 2.8. Quantification of etoposide in pharmacokinetic studies

Quantification of etoposide in plasma samples was performed on an API 4000<sup>TM</sup> LC/MSMS System from AB SCIEX (Ontario, Canada). Briefly, plasma samples were precipitated with acetonitrile after wash-out from the end-to-end capillaries. Chromatographic separation was carried out using an Acquity UPLC BEH C18 column (1.7  $\mu$ m, 2.1 mm  $\times$  50 mm). Gradient elution was performed at 50 °C with 0.01M ammonium acetate (mobile phase A) and acetonitrile (mobile phase B). Starting conditions were 5 % B for 0.25 minutes, then a linear gradient to 95% B was applied over 1.25 minutes, followed by an isocratic hold at 95% B for 0.5 min before re-equilibration at 5% B. Total run time was 2.5 min and a flow rate of 0.6 mL/min was applied.

The LC-MS/MS was operated in positive ion mode using the TurboIonSprayTM-interface (electrospray ionization), and was optimized for the quantification of etoposide, applying multiple reaction monitoring (m/z  $587.2 \rightarrow \text{m/z} 381$ ).

Incurred samples were quantified against calibration curves prepared in blank rat plasma. Independent quality control samples were included to evaluate accuracy (between 80 and 120% of the nominal

value) of the analytical run. The concentrations were correlated linearly, with a  $1/x^2$  weighing, with the MS response between 1.00 and 10000 ng mL<sup>-1</sup>.

#### 2.9. Population Pharmacokinetic analysis

Population pharmacokinetic analysis was performed using Monolix 2018R2 (Lixoft SAS, Antony, France) based on a two-compartment population pharmacokinetic model with linear first order elimination and an oral depot compartment with subsequent first order absorption. Population pharmacokinetic parameter estimates were generated using the stochastic approximation expectation-maximization (SAEM) algorithm. Modeling was performed using the clearance parameterization assuming a lognormal distribution of individual parameters. The individual parameter estimates for the *i*th subject were modeled according to equation 2.

$$\theta_i = \theta_{\text{pop}} \cdot e^{\eta_{\theta,i}} \tag{2}$$

where  $\theta_i$  is the individual parameter estimate for the *i*th subject,  $\theta_{pop}$  is the typical population parameter estimate and  $\eta_{\theta,i}$  is assumed to be the random individual deviation for the *i*th subject for a particular population parameter  $\theta$ . The clearance parametrization included the volume of the central compartment (V<sub>1</sub>), the elimination clearance (CL), the volume of the peripheral compartment (V<sub>2</sub>), and the inter-compartmental flow between the central and the peripheral compartment (Q<sub>2</sub>). Oral administration was modeled using a dosing compartment and subsequent first order absorption. The final model included covariate effects, which partly explained differences observed between animals assigned to the different formulation groups. Forward inclusion of covariates was judged based on the decrease in objective function value expressed as -2 log likelihood (-2LL) and Akaike's information criterion (AIC). Covariate selection was guided by physiological plausibility and

statistical significance (P < 0.05). Covariate effects of the final population model included the presence of zosuquidar on F and the presence of experimental matrix (referred as formulation G-matrix) on F and  $k_a$ . The final model estimated inter-individual variability for F,  $k_a$ ,  $V_1$  and CL. Residual error was accounted for by a combined (additive and proportional) error model (Equation 3).

$$\log(Y_{ij}) = \log(c_{\text{pred},ij}) + (a + b \cdot \log(c_{\text{pred},ij}))\epsilon_{ij}$$
(3)

where the *j*th observation of the *i*th subject deviates from the *j*th prediction of the *i*th subject,  $c_{pred,ij}$ , by an additive term, a, and a proportional term, b.  $\epsilon_{ij}$  was assumed to be the random variable for the *j*th concentration of the *i*th individual, sampled from a distribution with zero as a mean and a variance of  $\sigma^2$ . Individual Bayesian estimates were used to calculate mean AUC<sub>0- $\infty$ </sub> per study cohort. Individual AUC<sub>0- $\infty$ </sub> values (AUC<sub>0- $\infty$ ,i) were calculated as shown in equation 4.</sub>

$$AUC_{0-\infty,i} = \frac{F_{i} \cdot D}{CL_{i}}$$
 (4)

2.10. Statistics

The results of *in vitro* studies were obtained from at least three experiments and presented as mean values  $\pm$  SEM. Caco-2 cell experiments were conducted in three independent cell passages and values are presented as mean values  $\pm$  SEM. The results of the *in vivo* pharmacokinetic studies were obtained from 5 or 6 rats per study cohort and data are presented as mean values  $\pm$  SEM. Statistical analysis was performed using GraphPad Prism 7.01 from GraphPad Software, LLC (San Diego, CA, USA). One-way ANOVA test followed by Tukey's multiple comparisons test were selected for multiple comparisons. P value < 0.05 was considered statistically significantly different from control.

Moreover, dose-proportionality has been assessed by plotting  $AUC_{0-\infty}$  as a function of oral etoposide doses and linear regression analysis was performed.

#### 3. Results

3.1. Transepithelial flux of etoposide across Caco-2 cells

Etoposide transport across Caco-2 monolayers was investigated, and in the following Figure 1, the A-B and B-A flux dependent on P-gp is shown. The A-B flux dependent on P-gp shows a gradual increase as a function of concentration and at higher concentrations the flux is relatively linear as a function of concentration in the apical donor solution (Fig. 1A). In the B-A direction, the flux of etoposide across Caco-2 cells monolayers can be described by Michaelis-Menten like kinetics where the flux becomes saturated with increasing concentration in the basolateral medium. The resulting kinetical parameters were estimated at  $257 \pm 32 \,\mu\text{M}$ ,  $199 \pm 17 \,\text{pmol cm}^{-2} \,\text{min}^{-1}$ , and  $1.7 \pm 0.2 \,\text{for}$   $K_{m,app}$ ,  $J_{P-gp,max}$ , and the Hill coefficient, respectively.

3.2. Etoposide did not precipitate in formulations containing high percentages of ethanol

Different formulations of etoposide were prepared using 44% or 57% (v/v) ethanol, 2-10% (w/v) pluronic<sup>®</sup> F-127, and 0-15% (w/v) PVP/VA (Table 1). Etoposide in formulations containing 44% (v/v) ethanol either contained low concentration of etoposide such as 9 mg mL<sup>-1</sup> (Formulation A), which was not sufficient to perform our study or precipitated after overnight incubation such as Formulation B (Fig. 2). Etoposide formulations (C-G) showed no signs of etoposide precipitation after overnight incubation; e.g. Formulation G as shown in Figure 2. Etoposide solubility in these formulations containing 57% (v/v) ethanol was higher than in formulation A and B. Formulation D showed that 6% (w/v) of the surfactant was required to dissolve 15 mg mL<sup>-1</sup> etoposide in PVP/VA-

free formulation. Formulations A, C, and E-G were designed to contain 5-15% (w/v) PVP/VA as a potential precipitation inhibitor. Formulation G consisting of 10% (w/v) of pluronic<sup>®</sup> F-127 and PVP/VA, 57% ethanol, and water could solubilize an amount of etoposide corresponding to a 100-fold increase compared to the aqueous solubility. Further studies were conducted to investigate whether etoposide precipitates after the addition of different formulations to FaSSIF.

3.3. Etoposide did not precipitate from Formulation G after dilution in fasted state simulated intestinal fluid

Formulations C-E showed a fast etoposide precipitation (less than 30 min) after dilution in FaSSIF. Formulation F started to precipitate after approx. one hour and reached similar levels of absorbance values as C-E at 90 min. Therefore, formulations C-F were only prepared and investigated once. Formulation G showed no sign of etoposide precipitation for 120 min (Fig. 3). After 120 min, etoposide started to precipitate indicating that the matrix of formulation G was able to maintain etoposide in a solubilized form in FaSSIF for two hours (Fig. 3), which is the period that likely covers the absorption phase of etoposide in rats. Equal amounts of pluronic® F-127 and PVP/VA at 10% (w/v) were required to maintain etoposide in a solubilized form when diluted with FaSSIF. Among the investigated formulations, formulation G was stable in FaSSIF and the next step was to investigate if the formulation G would retain etoposide.

3.4. Etoposide release was similar from different surfactant-containing solutions and matrix of formulation G

As shown in Figure 4, simultaneous etoposide and glycine release from different pluronic<sup>®</sup> F-127-containing solutions and formulation G to receiver-release media increased time dependently. The release of etoposide and glycine from different pluronic<sup>®</sup> F-127-containing formulations and from formulation G was similar to the release in the control buffer i.e. without surfactant. Moreover, there was no statistically significant difference between the slopes of the time-dependent release of etoposide or glycine compared to control. The presence of non-radiolabeled etoposide in formulation G did not affect the release of radiolabeled etoposide during the course of the experiment.

# 3.5. Etoposide population pharmacokinetics in WT male Sprague-Dawley rats after intravenous and oral administration

Pharmacokinetic data available included 321 concentration-time points collected from 35 male WT Sprague-Dawley rats. The PK profile af intravenous administration of etoposide is shown in figure 5, illustrating a fast distribution phase followed by a slower elimination phase. Data points at 4 h post intravenous administration of etoposide are not shown in Figure 5 as the plasma concentration values were below the limit of quantification (LOQ) at this time point, and only three plasma-concentrations had values above LOQ at 6 h. Etoposide pharmacokinetic profiles after oral administration of etoposide-containing solutions were best described by a two-compartment structural model with linear elimination and first-order absorption (Fig. 6). Subsequently, a covariate model was developed to account for the inter-individual variability arising from the experimental design. The introduction of zosuquidar dose as a covariate on the oral bioavailability F, and matrix-G presence as a covariate on F as well as on the absorption rate constant (ka) significantly improved the model fit. After covariate inclusion, the unexplained inter-individual variability for F and ka, calculated as the square root of the exponential variance of  $\eta$  minus 1, decreased from 153% for F and 59.7% for ka to 15.9%

and 53.5%, respectively, from the base structural model to the final covariate model ( $\Delta 138\%$  for F and  $\Delta 6.15\%$  for  $k_a$ ). Estimated population pharmacokinetic parameters, precision of the parameter estimates and objective function values of both the base structural model and the final covariate model are presented in Table 2. Empirical Bayesian estimates were used to calculate  $AUC_{0-\infty}$  and dose normalized  $AUC_{0-\infty}$ , dose normalized  $AUC_{0-\infty}$ ,  $t_{1/2}$ ,  $t_{max}$  and  $C_{max}$  are presented in Table 3. Rats pretreated with zosuquidar showed the largest etoposide exposure ( $AUC_{0-\infty}$  of 4511 ng h mL<sup>-1</sup> kg). Dose-proportional etoposide exposure was observed for the 20, 50, and 100 mg kg<sup>-1</sup> dosing cohorts receiving etoposide prepared in the matrix of formulation G (i.e. 10% of pluronic® F-127 and PVP/VA, 57% ethanol, and water), and R square was equal to 0.99 when the AUC was plotted as a function of dose (supplementary figure S1). However, the F,  $k_a$ ,  $AUC_{0-\infty}$ , and  $C_{max}$  were significantly lower when the rats were dosed with etoposide 20 mg kg<sup>-1</sup> dissolved in the matrix of formulation G compared to the control group. Etoposide oral bioavailability significantly increased when the rats were pretreated with zosuquidar. The oral pharmacokinetic profile showed that the oral absorption of etoposide was slower in matrix-based formulations as was also apparent from the decreased  $k_a$  values.

#### 4. Discussion

In the present study, a stable formulation containing high concentration of etoposide and ethanol (57%) was developed using a surfactant without P-gp inhibiting properties. After oral administration of etoposide in this formulation, no increased bioavailability related to P-gp saturation could be shown, illustrating the practical difficulties in saturating P-gp mediated transport of low soluble drug substances for increasing the oral absorption through a formulation approach.

To investigated if the transport of etoposide was saturable, we used the approach described by Troutman and Thakker (Troutman and Thakker, 2003a), in which the net flux due to P-gp mediated

transport is estimated by subtracting the flux under P-gp inhibited conditions. We found that the B-A transport was saturable with kinetical parameters similar to the ones described by Troutman and Thakker in Caco-2 cells, for  $K_{m,app}$  257 vs. 461  $\mu M$ , and for  $J_{max}$  199 vs. 354 pmol cm<sup>-2</sup> min<sup>-1</sup> (Troutman and Thakker, 2003a). Makhey et al. found a similar K<sub>m</sub> value of 113 µM in Caco-2 cells and 94-119 µM in stripped rat intestinal tissue (Makhey et al., 1998). Troutman and Thakker estimated a higher K<sub>m</sub> value of 1360 µM for the A-B transport direction (Troutman and Thakker, 2003a), however this value was outside the concentration range that could be investigated in our setup. Even though the B-A transport appears saturable and while it is more difficult to be assessed from the A-B transport, studies in wild-type and knock-out rats clearly show that the apically located P-gp is highly attenuating the oral etoposide absorption (Al-Ali et al., 2018a). Considering the above mentioned K<sub>m</sub> values, generally of approximately 100-500 µM, an intestinal concentration of 10 times these values would likely be required to fully saturate P-gp mediated transport by etoposide itself, corresponding to approximately 5000 µM for the worst case scenario. A solubility higher than that could be achieved with formulation G (16 mg mL<sup>-1</sup> (27183 µM)) containing 10% of pluronic® F-127 and 10% PVP/VA. 16 mg ml<sup>-1</sup> is approximately 100-fold higher than the aqueous solubility of etoposide (Beig et al., 2015; Darwish et al., 1989). Pluronic® F-127 forms micelles that have the capacity to solubilize lipophilic drug substances e.g. meso-tetraphenyl porphine (mTPP) (Sezgin et al., 2007), rofecoxib (Ahuja et al., 2007), ibuprofen (Wan et al., 2010), paclitaxel, and lapatinib (Kelishady et al., 2015). The reported critical micelle concentration (CMC) values of pluronic® F-127 were 1, 0.1, and 0.025% (w/v) at 25, 30, and 35°C (Alexandridis and Hatton, 1995), respectively. Etoposide in micelles could be retained from permeation and hence the oral absorption could be decreased, which has been reported with 25% polysorbate 20 (Al-Ali et al., 2018a). However, the presence of different concentrations of pluronic<sup>®</sup> F-127 did not affect the *in vitro* release of etoposide and glycine compared to the release from a surfactant-free formulation. Similarly, 1% (w/v) pluronic®

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430 F-127, which is above the CMC value, did not affect the release of the lipophilic drug rofecoxib

(Ahuja et al., 2007) (Log P 2.56) (Chemicalize, 2018).

Previous pharmacokinetic studies in rats have shown that  $t_{max}$  of etoposide exposure was between 0.25-1.75 h (Al-Ali et al., 2018a; Li et al., 2009; Zhao et al., 2013), therefore the formulation should maintain etoposide in its solubilized form for two hours when diluted in FaSSIF. This period was considered sufficient for further *in vivo* studies. In formulation G, solubilized etoposide did not precipitate for two hours when diluted with FaSSIF. Thus, pluronic® F-127 probably had two functions: i) enhanced the solubility of etoposide, and ii) decreased the precipitation rate of etoposide as it was also suggested by (Li et al., 2012; Xu and Dai, 2013), thereby stabilizing the formulation in FaSSIF. Importantly, it seems that a balance between pluronic® F-127 and PVP/VA concentrations (i.e. 10% of each) in the formulation was needed to achieve these formulation characteristics. Thus, if an intestinal dilution of 3-10 is expected after oral administration of a 16 mg mL<sup>-1</sup> etoposide formulation, and initial estimated intestinal concentration of 2718 – 9061  $\mu$ M could be obtained, which could be able to saturate P-gp assuming that etoposide remains in solution.

In rats receiving 100 mg kg<sup>-1</sup> of etoposide in formulation G, a higher AUC<sub>0-∞</sub> was obtained compared to rats receiving 20 mg kg<sup>-1</sup> etoposide in a 57% ethanol solution. Even though the systemic exposure of etoposide increased with higher doses, the absolute bioavailability decreased, and this does not seem to involve P-gp saturation by etoposide as the absolute bioavailability should then increase. However, zosuquidar enhanced the oral absorption and bioavailability of etoposide. Yet, in the presence of 20 mg kg<sup>-1</sup> zosuquidar, only 34.5% of the etoposide dose reached the systemic circulation, thus zosuquidar itself most likely did not cause full inhibition of intestinal P-gp.

Surprisingly, the absolute oral bioavailability of etoposide was low compared to our previous study (Al-Ali et al., 2018a). Al-Ali and coworkers reported that the oral bioavailability of etoposide was 27

± 5% (Al-Ali et al., 2018a). Zhao and co-workers reported an oral bioavailability of etoposide of 25 ± 7% in WT male Sprague-Dawley rats dosed with 12 mg kg<sup>-1</sup> etoposide suspended (1.5 mg mL<sup>-1</sup>) in 0.5% sodium carboxymethyl cellulose (Zhao et al., 2013). Li and co-workers reported an oral bioavailability of  $7.5 \pm 1.8\%$  in WT male Sprague-Dawley rats after oral administration of a 6 mg kg<sup>-1</sup> <sup>1</sup> etoposide solution prepared as an injectable formulation (specific composition not specified) (Li et al., 2009). In the present study, it was not clear why the oral bioavailability of etoposide was low in the control group, however, besides the known variabilities observed between animal studies (Festing and Altman, 2002), one could speculate that the 57% of ethanol could be the cause, since etoposide could precipitate in the intestinal lumen. In the previous study by Al-Ali et al, the oral bioavailability of etoposide (27%) was obtained after administration of 20 mg kg<sup>-1</sup> in 40% ethanol (2 mg ml<sup>-1</sup>) administered with a dosing volume of 10 mL kg<sup>-1</sup> (Al-Ali et al., 2018a). In the present study an etoposide solution (2.86 mg mL<sup>-1</sup>) in 57% (v/v) ethanol at a dose of 20 mg kg<sup>-1</sup> etoposide and a dosing volume of 7 mL kg<sup>-1</sup> was used, thus approximately similar absolute amounts of ethanol were administered in the two studies, but the concentration of etoposide and the amount of water differ, with concentration of etoposide in the previous study being lower and water amount higher. This could affect the susceptibility of etoposide precipitation in the solution used here to be higher. Ethanol is rapidly absorbed in rats with a t<sub>max</sub> less than 60 min and 50% disappearance of ethanol from the stomach after 60 min (Siegers et al., 1972). If etoposide has indeed precipitated, this could explain the low bioavailability. Population analysis indicated that formulation G decreased both the oral bioavailability and the absorption rate while a clear increase in oral bioavailability was quantified in the presence of zosuguidar administration. Introduction of these covariate effects on the respective parameters of the population pharmacokinetic model significantly decreased the objective function values (OFVs) and improved the model fit upon inspection of diagnostic plots (see Table 2). It has been described earlier that 25% (v/v) polysorbate 20 decreased etoposide oral absorption, when

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similar doses of 20 mg kg<sup>-1</sup> of etoposide were co-administered in rats (Al-Ali et al., 2018a). In the study reported by Al-Ali et al., dialysis experiments showed that polysorbate 20 at 25% (v/v) abolished etoposide release across polycarbonate membranes (Al-Ali et al., 2018a). In contrast, the present study showed that etoposide release from the matrix across polycarbonate membrane was not affected by the presence of different components in the formulation such as pluronic<sup>®</sup> F-127. *In vivo*, this points to an effect of the high ethanol concentration rather than incomplete release from colloidal structures present in the intestinal lumen.

#### 5. Conclusion

In conclusion, an oral formulation of high-concentration of etoposide, which maintained etoposide in a solubilized form under short-term storage conditions and when diluted with simulated intestinal fluid was developed. Administration of increasing etoposide doses using this formulation-matrix enhanced the plasma exposure of etoposide dose-proportionally. However, the applied doses were not able to saturate P-gp, and the absolute absorption fraction decreased as a function of increasing dose. To saturate intestinal P-gp by etoposide in rats, oral formulations maintaining high concentrations of etoposide in solution are needed, yet the present study is a starting point for developing formulation approaches using other drug candidates aimed at increasing the oral absorption of P-gp substrates and illustrates the difficulties in developing formulations aimed at saturating intestinal P-gp transport.

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draft preparation, AAAA and CUN; writing—review and editing, AAAA, LS, LD, IP, AV, JS, RH, and CUN; formal analysis, AAAA, LS, AV, and CUN; supervision, RH and CUN; project administration, CUN.

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### 673 Figures Legends:

- Figure 1. Transepithelial P-gp dependent flux of etoposide across Caco-2 cell monolayers. The
- steady-state P-gp dependent flux (pmol cm<sup>-2</sup> min<sup>-1</sup>) of etoposide across Caco-2 cells grown on
- 676 permeable support for 24-28 days was studied as a function of etoposide concentration (C<sub>d</sub>, μM) in
- the donor solution. The A-B transport (A) and B-A (B) transport was measured in 3 cell passages. In

B, the line is obtained by fitting experimental points to Eq. 1 described in Materials and Methods.

Values are given as mean  $\pm$  SEM.

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Figure 2. Pictures of etoposide formulations after 15 hours of storage at room temperature.

Formulation B contained 12 mg mL<sup>-1</sup> etoposide, 10% (w/v) of pluronic<sup>®</sup> F-127 in 44% (v/v) ethanol.

Formulation G contained 16 mg mL<sup>-1</sup> etoposide, 10% (w/v) of pluronic<sup>®</sup> F-127, and 10% (w/v) of

PVP/VA in 57% (v/v) ethanol.

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Figure 3. Absorbance measurments at 400 nm of etoposide formulations added to fasted state

simulated intestinal fluid (FaSSIF) in a ratio of (Formulation:FaSSIF, 1:2) as a function of time.

Etoposide formulations were composed as shown in Table 1. The measurments were performed at

room temperature. For formulation G, n=4 and as mean  $\pm$  SEM, for other formulations n=1.

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Figure 4. Time dependent release of etoposide and glycine from different formulations across

**0.03 μm polycarbonate membrane.** Donor solutions of <sup>3</sup>H-etoposide and <sup>14</sup>C-glycine were prepared

in Hanks Balanced Salt Solution (HBSS) buffer supplemented with 10 mM HEPES and adjusted to

pH 7.40 ± 0.05 (Control), or in different formulation-matrix containing 10% (w/v) PVP/VA, 57%

(v/v) ethanol, and pluronic<sup>®</sup> F-127 (PF127) at 1.5, 3, or 10% (w/v), referred as Matrix-PF127 1.5%,

Matrix-PF127 3%, or Matrix-PF127 10%, respectively, or mixed with formulation G which contained

15-16 mg mL<sup>-1</sup> etoposide, 10% (w/v) of PF127 and PVP/VA, and 57% (v/v) ethanol. Receiver-release

media were HBSS buffer supplemented with 10 mM HEPES and adjusted to pH  $6.50 \pm 0.05$  for all

conditions, except in formulation G condition where the receiver-release media was the matrix of

formulation G (i.e. 10% (w/v) of PF127 and PVP/VA, and 57% ethanol, and q.s. water but without etoposide). Experiments were performed at 37  $^{\circ}$ C and shaking mode 220 rpm. Data are expressed in mean  $\pm$  SEM from 3-4 independent membranes and as one membrane per experiment.

Figure 5. Plasma concentration time profile of etoposide after intravenous administration of 5 mg kg<sup>-1</sup> etoposide to wild-type male Sprague-Dawley rats. Each data point is shown as mean  $\pm$  SEM from 3-6 rats.

Figure 6. Plasma concentration time profiles of etoposide after oral administration of different doses of etoposide in wild-type male Sprague-Dawley rats. A) Etoposide was administered orally at a dose of 20 mg kg<sup>-1</sup> in 57% (v/v) ethanol solution (Control), or at increasing doses of etoposide dissolved in matrix at 20, 50, and 100 mg kg<sup>-1</sup> etoposide. The matrix was consisted of 10 % (w/v) pluronic<sup>®</sup> F-127 and PVP/VA, and 57% (v/v) ethanol, and q.s. water. At the highest oral dose, the formulation is referred as formulation G. B) Etoposide was administered orally as control after the rats were received an oral dose 20 mg kg<sup>-1</sup> of zosuquidar. Each data point is shown as mean  $\pm$  SEM from 5-6 rats. The solid lines are only connecting the data points.

- Supplementary Figure S1. AUC after oral administration as a function of dose.
- Each data point is shown as mean  $\pm$  SEM from 5-6 rats.

Table 1: Composition of oral formulations of etoposide. (nd : not determined,  $\checkmark$ : Yes,  $\div$  : no). a: (Li et al., 2012; Xu and Dai, 2013)

	Formulations						Function			
Composition	A	В	C	D	E	F	G			
Etoposide (mg mL <sup>-1</sup> )	9	12	12	15	15	15	16	API, P-gp substrate		
Pluronic <sup>®</sup> F-127 (% w/v)	4.7	10	6	6	2	6	10	Surfactant, precipitation inhibitor <sup>a</sup>		
PVP/VA (% w/v)	5	-	15	-	5	10	10	Precipitation inhibitor		
Ethanol (% v/v)	44	44	57	57	57	57	57	Co-solvent/solvent		
Ultra-purified water	qs	qs	qs	qs	qs	qs	Qs	Solvent		
Stable under storage for 15 h	<b>√</b>	÷	$\checkmark$	$\checkmark$	$\checkmark$	$\checkmark$	$\checkmark$			
Stable for 2 h after dilution with FaSSIF	nd	nd	÷	÷	÷	÷	<b>√</b>			

Table 2: Population pharmacokinetic parameter estimates of the base structural model and the final covariate model. Precision of the parameter estimates is reported as relative standard error (RSE%). F = oral bioavailability,  $k_a$  = absorption rate, V1 = volume of the central compartment, V2 = volume of the peripheral compartment, CL = elimination clearance, Q2 = intercompartmental clearance,  $\beta_{F,FORM}$  = categorical covariate effect of formulation G presence on F,  $\beta_{F,ZOSU}$  = categorical covariate effect of zosuquidar presence on F,  $\beta_{K_a,FORM}$  = categorical covariate effect of formulation G presence on  $k_a$ ,  $k_a$  = additive error model term,  $k_a$  = proportional error model term, OFV = objective function value, -2LL = minus 2 times log likelihood, AIC = Akaike information criterion.

	Base structural model	Final covariate model					
Fixed effects [RSE%]							
F (%)	6.76 [24.2]	3.92 [16.7]					
ka (h-1)	2.69 [13.1]	4.54 [20.2]					
V1 (L kg <sup>-1</sup> )	3.63 [18]	2.91 [18.7]					
V2 (L kg <sup>-1</sup> )	3.18 [12.2]	3.78 [17.9]					
CL (L h-1 kg -1)	1.61 [4.62]	1.55 [10.1]					
Q2 (L h <sup>-1</sup> kg <sup>-1</sup> )	6.56 [13.6]	6.98 [18.6]					
$oldsymbol{eta}_{F,FORM}$	-	-0.51 [37.9]					
$\beta_{F,ZOSU}$	-	2.17 [7.04]					
$\beta_{k_a,FORM}$	-	-0.713 [34.8]					
Random effects (SD) [RSE%]							
F	1.1 [13.4]	0.158 [28.1]					
ka	0.552 [20.6]	0.502 [23.2]					
V1	0.924 [13]	0.678 [15]					
CL	0.122 [35.6]	0.118 [38.8]					
Error model [RSE%]							
a	0.01 [14.1]	0.0115 [14.5]					
b	0.132 [9.34]	0.135 [10.9]					
OFV	•						
-2LL	-665.17	-734.78					
AIC	-641.17	-704.78					

Table 3: Estimated pharmacokinetic parameters after intravenous and oral administration of different doses of etoposide in wild-type male Sprague-Dawley rats. Matrix solution consisted of 10 % (w/v) pluronic<sup>®</sup> F-127, 10% (w/v) PVP/VA, 57% (v/v) ethanol, and q.s. water. Individual Bayesian (post hoc) estimates were used to calculate mean AUC<sub>0-∞</sub>. Data are expressed as mean  $\pm$  SEM except for  $t_{max}$  that is expressed as the median [Q1; Q3] (25% and 75% percentile). No random effects were estimated for Q and V<sub>2</sub>. Fixed effects were estimated as Q = 6.98 mL h<sup>-1</sup> kg<sup>-1</sup>, V<sub>2</sub> = 3778 mL kg<sup>-1</sup>. Statistical significance was tested by one-way ANOVA followed by Tukey's multiple comparisons test. When all the groups, except the group of rats pre-dosed with zosuquidar and the group of rats receiving i.v. administration, were included in the comparison, (\*) referred to P < 0.05 compared to control. When all the groups, except the group of rats receiving i.v. administration, were included in the comparison, (†) referred to P < 0.05 compared to control.

	Study cohorts						
<b>Etoposide dose</b>	20 mg kg <sup>-1</sup>	20 mg kg <sup>-1</sup>	50 mg kg <sup>-1</sup>	100 mg kg <sup>-1</sup>	20 mg kg <sup>-1</sup>	5 mg kg <sup>-1</sup>	
Condition	Control				Zosuquidar		
<b>Etoposide solution</b>	57% EtOH	Matrix	Matrix	Matrix	57% EtOH	57% EtOH	
<b>Cohort Size</b>	6	5	6	6	6	6	
Administration route	p.o.	p.o.	p.o.	p.o.	p.o.	i.v.	
F (%)	$4.0 \pm 0.13$	$2.4 \pm 0.02*$	$2.4 \pm 0.07*$	$2.2 \pm 0.09*$	$34.5 \pm 0.18^{\dagger}$	$100 \pm 0$	
ka (h <sup>-1</sup> )	$6.40 \pm 0.94$	$2.29 \pm 0.41 ^{*\dagger}$	$2.36\pm0.35^{*\dagger}$	$2.32\pm0.32^{*\dagger}$	$3.43\pm0.41^{\dagger}$	-	

CL (mL h <sup>-1</sup> kg <sup>-1</sup> )	$1547 \pm 28$	$1533 \pm 6.9$	$1503 \pm 24$	$1587 \pm 39$	$1550 \pm 43$	$1636 \pm 85$
$V_1 \ (mL \ kg^{\text{-}1})$	$3830 \pm 574$	$4263 \pm 193$	$4143 \pm 315$	$4953 \pm 640$	$2996 \pm 436$	$809 \pm 50$
$AUC_{0\text{-}\infty} (ng \ h \ mL^{\text{-}1})$	$518.8 \pm 25$	$307.2 \pm 3.5*$	$816.5 \pm 38*$	1525 ± 86*	$4511 \pm 384^{\dagger}$	$3096 \pm 155$
$AUC_{0-\infty}/D$ (h mL <sup>-1</sup> kg)	$25.9 \pm 1.3$	$15.4 \pm 0.2$	$16.3 \pm 0.8$	$14.2 \pm 0.9$	$225.5 \pm 19.2$	$619.2 \pm 31.0$
t½ (h)	$1.73 \pm 0.27$	$1.93 \pm 0.08$	$1.91 \pm 0.14$	$2.18 \pm 0.31$	$1.36 \pm 0.23$	$0.35 \pm 0.02$
t <sub>max</sub> (h)	0.375 [0.25-0.5]	0.625 [0.44-0.75]	0.75 [0.25-1.06]	0.75 [0.5-1.25]	0.5 [0.5-0.81]	-
C <sub>max</sub> (ng mL <sup>-1</sup> )	191 ± 19	63 ± 4*	$169 \pm 17$	$266 \pm 38*$	$1542\pm190^{\dagger}$	-

















